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(21) International Application Number: PCT/GB99/02914 (22) International Filing Date: 3 September 1999 (03.09.99) (30) Priority Data: 60/099,157 4 September 1998 (04.09.98) US (71) Applicant (for all designated States except US): POWDER-JECT RESEARCH LIMITED [GB/GB]; The Oxford Science Park, 4 Robert Robinson Avenue, Oxford OX4 4GA (GB). (72) Inventor; and (75) Inventor/Applicant (for US only): KWON, Sung-Yun [US/US]; 6511 Dumbarton Circle, Fremont, CA 94555 (US). (74) Agent: WOODS, Geoffrey, Corlett; J.A. Kemp & Co., 14 South Square, Gray's Inn, London WC1R 5LX (GB).		(81) Designated States: AE, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, DE, DK, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG). Published <i>With international search report.</i>
(54) Title: MONITORING METHODS USING PARTICLE DELIVERY METHODS (57) Abstract Methods for sampling an analyte present in a biological system are provided. The methods entail use of particle delivery methods to obtain a sample of an analyte of interest from the system.		

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MONITORING METHODS USING PARTICLE DELIVERY METHODS

Technical Field

5 This invention relates generally to methods of monitoring the presence and/or concentration of target analytes in an aqueous biological system. More particularly, the invention relates to methods for determining the presence, for example measuring the concentration, of one or more analytes in a transdermally extracted sample. One important application of the invention involves a sampling method for monitoring
10 blood glucose using non-invasive or minimally invasive sampling techniques.

Background

 A number of tests are routinely performed on humans to evaluate the amount or existence of substances present in blood or other body fluids. These tests typically
15 rely on physiological fluid samples removed from a subject, either using a syringe or by pricking the skin. One particular test entails self-monitoring of blood glucose levels by diabetics.

 Diabetes is a major health concern, and treatment of the more severe form of the condition, Type I (insulin-dependent) diabetes, requires one or more insulin
20 injections per day. Insulin controls utilization of glucose or sugar in the blood and prevents hyperglycemia which, if left uncorrected, can lead to ketosis. On the other hand, improper administration of insulin therapy can result in hypoglycemic episodes, which can cause coma and death. Hyperglycemia in diabetics has been correlated with several long-term effects, such as heart disease, atherosclerosis,
25 blindness, stroke, hypertension and kidney failure.

 The value of frequent monitoring of blood glucose as a means to avoid or at least minimize the complications of Type I diabetes is well established. According to the National Institutes of Health, glucose monitoring is recommended 4-6 times a day. Patients with Type II (non-insulin-dependent) diabetes can also benefit from
30 blood glucose monitoring in the control of their condition by way of diet and exercise.

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Conventional blood glucose monitoring methods generally require the drawing of a blood sample (e.g., by finger prick) for each test, and a determination of the glucose level using an instrument that reads glucose concentrations by electrochemical or colorimetric methods. Type I diabetics must obtain several finger
5 prick blood glucose measurements each day in order to maintain tight glycemic control. However, the pain and inconvenience associated with this blood sampling, along with the fear of hypoglycemia, has lead to poor patient compliance, despite strong evidence that tight control dramatically reduces long-term diabetic complications. In fact, these considerations can often lead to an abatement of the
10 monitoring process by the diabetic.

Summary of the Invention

The present invention provides a method for sampling an analyte present in a biological system. More especially, the invention provides a method for sampling an
15 analyte present beneath a target skin or mucosal surface of an individual, said method comprising:

- (a) accelerating particles into and/or across said target surface, wherein acceleration of said particles into or across the target surface is effective to allow passage of a fluid sample from
20 beneath the target surface to the target surface; and
- (b) determining the presence of said analyte in said fluid sample.

The invention also provides use of an inert material for the manufacture of a particulate composition for sampling an analyte present beneath a target skin or
25 mucosal surface of an individual by such a method. The method can be used to determine, for example qualitatively or quantitatively, the presence of an analyte of interest in the biological system. The method can also be used to determine the amount or concentration of the analyte of interest. In addition, the method can be used to continually or continuously measure the concentration of the analyte.

30 The method entails accelerating particles into and/or across a target surface of the biological system such that the particles allow a quantity of an analyte to pass

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from beneath the target surface. The analyte can then be contacted with a sensing apparatus to derive a raw detectable signal therefrom, wherein the raw signal is either indicative of the presence of the analyte, or related to the analyte concentration. If desired, the analyte can be collected from the target surface prior to contact with the
5 sensing apparatus.

Sampling is carried out such that the analyte of interest is transdermally extracted from the biological system. In this regard, the terms "transdermal extraction" and "transdermally extracted" intend any non-invasive, or at least minimally invasive method of using particle delivery techniques to facilitate
10 extraction of an analyte from beneath a tissue surface, across skin or mucosal tissue for subsequent analysis on, or collection and analysis from the surface thereof. The terms further include any such extraction whether or not coupled with application of skin penetration enhancers, negative pressure (vacuum or suction), or other extraction technique.

15 Analyte (generally within a volume of fluid) which is extracted from the biological system is then either contacted directly with a sensing apparatus for obtaining a raw signal indicative of the presence and/or concentration of the analyte of interest, or collected and then contacted with the sensing apparatus. This raw signal can be obtained using any suitable sensing methodology including, for
20 example, methods which rely on direct contact of a sensing apparatus with the biological system, methods which rely on contact with a collected amount of the extracted analyte, and the like. The sensing apparatus used with any of the above-noted methods can employ any suitable sensing element to provide the raw signal including, but not limited to, physical, chemical, biochemical (e.g., enzymatic,
25 immunological, or the like), electrochemical, photochemical, spectrophotometric, polarimetric, colorimetric, radiometric, or like elements. In preferred embodiments of the invention, a biosensor is used which comprises an electrochemical sensing element.

The analyte can be any specific substance or component that one is desirous
30 of detecting and/or measuring in a chemical, physical, enzymatic, or optical analysis. Such analytes include, but are not limited to, toxins, contaminants, amino acids,

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enzyme substrates or products indicating a disease state or condition, other markers of disease states or conditions, drugs of recreation and/or abuse, performance-enhancing agents, therapeutic and/or pharmacologic agents, electrolytes, physiological analytes of interest (e.g., calcium, potassium, sodium, chloride, bicarbonate (CO₂), glucose, urea (blood urea nitrogen), lactate, and hemoglobin), lipids, and the like. In preferred embodiments, the analyte is a physiological analyte of interest, for example glucose, or a chemical that has a physiological action, for example a drug or pharmacological agent. As will be understood by the ordinarily skilled artisan upon reading the present specification, there are a large number of analytes that can be sampled using the present methods.

Accordingly, it is a primary object of the invention to provide a method for sampling an analyte present in a biological system. The analyte is typically present beneath a target skin or mucosal surface of an individual. The method entails the steps of accelerating sampling particles into and/or across a target surface. Acceleration of the sampling particles into or across the target surface is effective to allow passage of a quantity of the analyte (typically a fluid sample comprising the analyte) from beneath the target surface to the target surface. The sample can contain a diagnostic quantity of the analyte. The presence and/or amount or concentration of the analyte which is so extracted is then determined by direct contact with a sensing apparatus, or the analyte is collected from the target surface and then contacted with a sensing apparatus.

An advantage of the invention is that the sampling process can be readily practiced inside and outside of the clinical setting and without pain.

These and other objects, aspects, embodiments and advantages of the present invention will readily occur to those of ordinary skill in the art in view of the disclosure herein.

Description of the Figures

Figure 1 is a schematic diagram of the modified Franz cell used in Example 1 for *in vitro* glucose measurement.

Figure 2 is a plot of optical density of glucose solution in donor compartment

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and glucose extracted from three different skins in the *in vitro* study of Example 1.

Figures 3 to 5 are glucose tolerance test profiles on three individual subjects from the *in vivo* study of Example 2.

Figure 6 is a plot of optical density over venous glucose value from the study
5 of Example 2.

Detailed Description of the Preferred Embodiments

Before describing the present invention in detail, it is to be understood that this invention is not limited to particularly exemplified analytes or process
10 parameters as such may, of course, vary. It is also to be understood that the terminology used herein is for the purpose of describing particular embodiments of the invention only, and is not intended to be limiting.

All publications, patents and patent applications cited herein, whether *supra* or *infra*, are hereby incorporated by reference in their entirety.

15 It must be noted that, as used in this specification and the appended claims, the singular forms "a," "an" and "the" include plural referents unless the content clearly dictates otherwise. Thus, for example, reference to "a particle" includes a mixture of two or more such particles, reference to "an analyte" includes mixtures of two or more such analytes, and the like.

20

A. Definitions

Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which the invention pertains. Although a number of methods and materials similar
25 or equivalent to those described herein can be used in the practice of the present invention, the preferred materials and methods are described herein.

In describing the present invention, the following terms will be employed, and are intended to be defined as indicated below.

The term "analyte" is used herein in its broadest sense to denote any specific
30 substance or component that is being detected and/or measured in a physical, chemical, biochemical, electrochemical, photochemical, spectrophotometric,

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polarimetric, colorimetric, or radiometric analysis. A detectable signal can be obtained, either directly or indirectly, from such a material. In preferred embodiments, the analyte is a physiological analyte of interest (e.g., a physiologically active material), for example glucose, or a chemical that has a physiological action, for example a drug or pharmacological agent.

As used herein, the term "pharmacological agent" intends any compound or composition of matter which, when administered to an organism (human or animal), induces a desired pharmacologic and/or physiologic effect by local and/or systemic action.

As used herein, the term "sampling" means extraction of a substance from any biological system across a membrane, generally across skin or tissue. The membrane can be natural or artificial, and is generally animal in nature, such as natural or artificial skin, blood vessel tissue, intestinal tissue, and the like. A "biological system" thus includes both living and artificially maintained systems.

The term "collection reservoir" is used to describe any suitable containment means for containing a sample extracted from an individual using the methods of the present invention. Suitable collection reservoirs include, but are not limited to, pads, membranes, dipsticks, swabs, tubes, vials, cuvettes, capillary collection devices, and miniaturized etched, ablated or molded flow paths.

The terms "sensing device" or "sensing apparatus" encompass any device that can be used to measure the concentration of an analyte of interest. Preferred sensing devices for detecting blood analytes generally include electrochemical devices and chemical devices. Examples of electrochemical devices include the Clark electrode system (see, e.g., Updike et al. (1967) *Nature* 214:986-988), and other amperometric, coulometric, or potentiometric electrochemical devices. Examples of chemical devices include conventional enzyme-based reactions as used in the Lifescan® glucose monitor (see, e.g., U.S. Patent 4,935,346 to Phillips et al.). Detection and/or quantization of a chemical signal can also be carried out using readily available spectrophotometric monitoring devices.

The term "individual" encompasses any warm-blooded animal, particularly including a member of the class *Mammalia* such as, without limitation, humans and

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nonhuman primates such as chimpanzees and other apes and monkey species; farm animals such as cattle, sheep, pigs, goats and horses; domestic mammals such as dogs and cats; laboratory animals including rodents such as mice, rats and guinea pigs, and the like. The term does not denote a particular age or sex. Thus, adult and
5 newborn subjects, as well as fetuses, whether male or female, are intended to be covered.

B. General Methods

The invention relates to a method for sampling analytes present in a
10 biological system, typically a physiologically active material that is present beneath a target skin or mucosal surface of an individual. The method entails two general steps, a sampling step and a determination step. The sampling step can be generalized as follows. Small sampling particles are accelerated into and/or across a target surface. Acceleration and penetration of these particles is sufficient to create
15 passages which allow a quantity of an analyte of interest to flow, exude or otherwise pass from beneath the target surface to the target surface. The target surface generally has an overall size ranging from about 0.1 to about 5 cm².

The sampling particles typically comprise an inert material. The material may be dissolvable such as commonly employed physiologically acceptable soluble
20 materials including sugars (e.g., mannitol, sucrose, lactose, trehalose, and the like) and soluble or dissolvable polymers. Alternatively, the sampling particles can be comprised of insoluble materials such as starch, TiO₂, calcium carbonate, phosphate salts, hydroxy apatite, or even polymers or metals such as gold, platinum or tungsten. Insoluble materials are sloughed off with the normal skin or mucosal tissue renewal
25 process. Preferred materials are lactose, lactic acid, mannitol and polyethylene glycol such as PEG 8000.

If desired, the sampling particles can be coated with a locally active agent which facilitates the sampling step. For example, the sampling particles can be coated with a pharmacological agent such as a vasoactive agent or an anti-
30 inflammatory agent. The vasoactive agent is generally used to provide short-acting vasoactivity in order to maximize fluid access (maximize the analyte sample),

whereas the anti-inflammatory agent is generally used to provide local anti-inflammatory action to protect the target site. The sampling particles can also be coated with an osmotically active agent to facilitate the sampling process.

The sampling particles can be delivered from a needleless syringe system
5 such as those described in commonly owned International Publication Nos. WO 94/24263, WO 96/04947, WO 96/12513, and WO 96/20022, all of which are incorporated herein by reference. Delivery of sampling particles from these needleless syringe systems is generally practiced with particles having an approximate size generally ranging from 0.1 to 250 μm , preferably ranging from
10 about 10-70 μm . Particles larger than about 250 μm can also be delivered from the devices, with the upper limitation being the point at which the size of the particles would cause untoward pain and/or damage to the tissue.

The actual distance which the delivered particles will penetrate a target surface depends upon particle size (e.g., the nominal particle diameter assuming a
15 roughly spherical particle geometry), particle density, the initial velocity at which the particle impacts the surface, and the density and kinematic viscosity of the targeted skin tissue. In this regard, optimal particle densities for use in needleless injection generally range between about 0.1 and 25 g/cm^3 , preferably between about 0.9 and 1.5 g/cm^3 , and injection velocities generally range between about 100 and 3,000
20 m/sec. With appropriate gas pressure, particles having an average diameter of 10-70 μm can be readily accelerated through the nozzle at velocities approaching the supersonic speeds of a driving gas flow. Preferably, the pressure used when accelerating the particles will be less than 30 bar, preferably less than 25 bar and most preferably 20 bar or less.

25 Alternatively, the sampling particles can be delivered from a particle-mediated delivery device such as a so-called "gene-gun" type device which delivers particles using either a gaseous or electric discharge. An example of a gaseous discharge device is described in U.S. Patent No. 5,204,253. An explosive-type device is described in U.S. Patent No. 4,945,050. One example of a helium
30 discharge-type particle acceleration apparatus is the PowderJect XR[®] instrument (PowderJect Vaccines, Inc., Madison), WI, which instrument is described in U.S.

Patent No. 5,120,657. An electric discharge apparatus suitable for use herein is described in U.S. Patent No. 5,149,655. The disclosure of all of these patents is incorporated herein by reference.

After the sampling particles have been delivered into the target surface, a
5 fluid sample passes to the target surface. Typically this is a sample of, or containing, interstitial fluid. Passage of the fluid sample to the surface may be substantially instantaneous, or may occur over a period of time. The quantity of the sample which is released to the target surface may be varied by altering conditions such as the size and/or density of sampling particles and the settings of the apparatus used to delivery
10 the particles. The quantity of fluid released may often be small, such as $< 1\mu\text{l}$ which is generally sufficient for detection of the analyte.

Once the sample has passed to the target surface, the presence and/or amount or concentration of the analyte in the sample is determined. The sample may be contacted with a suitable sensing apparatus. This detection step can, of course, be
15 carried out in a continual or continuous manner. Continual or continuous detection allows for monitoring of target analyte concentration fluctuations. Furthermore, the sample believed to contain the analyte can first be collected from the target surface prior to being contacted with the sensing apparatus.

The sample may be collected from the target surface in a number of ways.
20 For example pads, membrane dipsticks, swabs, tubes, vials, curvettes, capillary collection devices and miniaturized etched, ablated or molded flow paths may be used as collection reservoirs. In a preferred aspect an absorbent material is passed over the target surface to absorb the fluid sample from the target surface for subsequent detection of the presence or amount of analyte. The absorbent material
25 may be in the form of a pad or swab. The absorbent material may additionally incorporate means to facilitate detection of the analyte such as an enzyme as described in more detail below.

The absorbent material may be applied to the target surface and subsequently contacted with a detection means to detect the analyte. The absorbent material may
30 comprise a hydrogel. Suitable gelling agents for forming a hydrogel include carbopol, calcium lactate, cellulose gum, klucel (HPMC), natrosol, gelatin powder or

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sodium alginate. The gelling agents may be present in water at levels such as 1% by weight in water.

The gel may be applied to the target surface and sufficient time allowed for analyte from the target surface to equilibrate in the gel prior to the detection step.

- 5 The time may be quite short such as from 30 seconds to 5 minutes. Detection may then be carried out by applying the sensing means to the gel such as by contacting a membrane containing a suitable enzyme system for the analyte with the hydrogel.

- The determination step can be generalized as follows. An initial step can entail obtaining a raw signal from a sensing device, which signal is related to a target
10 analyte present in the biological system. The raw signal can then be used directly to obtain an answer about the analyte, for example a yes or no answer relating to the presence of the analyte, or a direct measurement indicative of the amount or concentration of the extracted analyte. The raw signal can also be used indirectly to obtain information about the analyte. For example, the raw signal can be subjected
15 to signal processing steps in order to correlate a measurement of the sampled analyte with the concentration of that analyte in the biological system. Such correlation methodologies are well known to those skilled in the art.

- Detection may be carried out by any suitable method which allows for detection of a derived analyte. The analysis may be physical, chemical, biochemical,
20 electrochemical, photochemical, spectrophotometric, polarimetric, colorimetric or radiometric analysis.

- In order to facilitate detection of the analyte, an enzyme may be disposed on the active surface or portion of a sensing apparatus which is contacted with the extracted analyte (e.g., an extracted sample containing the analyte), or included
25 within one or more collection reservoirs which are used to collect the extracted analyte. Such enzymes must be capable of catalyzing a specific reaction with the extracted analyte (e.g., glucose) to the extent that a product of the reaction can be sensed (e.g., detected electrochemically from the generation of a current which current is detectable and proportional to the amount of the analyte which is reacted).
30 A suitable enzyme is glucose oxidase which oxidizes glucose to gluconic acid and hydrogen peroxide. The subsequent detection of hydrogen peroxide on an

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appropriate biosensor electrode generates two electrons per hydrogen peroxide molecule which create a current which can be detected and related to the amount of glucose entering the device. Glucose oxidase (GOx) is readily available commercially and has well known catalytic characteristics. However, other enzymes
5 can also be used, so long as they specifically catalyze a reaction with an analyte or substance of interest to generate a detectable product in proportion to the amount of analyte so reacted.

A number of other analyte-specific enzyme systems can be used in the methods of the invention. For example, when using a common biosensor electrode
10 that detects hydrogen peroxide, suitable enzyme systems can be used to detect ethanol (an alcohol oxidase enzyme system), or similarly uric acid (a urate oxidase system), cholesterol (a cholesterol oxidase system), and theophylline (a xanthine oxidase system). Hydrogels containing these analyte-specific enzyme systems can be prepared using readily available techniques familiar to the ordinarily skilled artisan.

15 Preferred sensing devices are patches that include an enzyme or other specific reagent which reacts with the extracted analyte of interest to produce a detectable color change or other chemical signal. The color change can be assessed by comparison against a standard to determine analyte amount, or the color change can be detected using standard electronic reflectance measurement instruments. One
20 such system is transdermal glucose monitoring system available from Technical Chemicals and Products, Inc (TCPI) of Pompano Beach, FL. Another suitable system is described in U.S. Patent No. 5,267,152 to Yang et al. (a device and method for measuring blood glucose concentration using near-IR radiation diffuse-reflection laser spectroscopy. Similar near-IR spectrometric devices are also described in U.S.
25 Patent No. 5,086,229 to Rosenthal et al. and U.S. Patent No. 4,975,581 to Robinson et al. U.S. Patent No. 5,139,023 to Stanley describes a blood glucose monitoring apparatus that relies on a permeability enhancer (e.g., a bile salt) to facilitate transdermal movement of glucose along a concentration gradient established between interstitial fluid and a receiving medium. U.S. Patent No. 5,036,861 to Sembrowich
30 describes a passive glucose monitor that collects perspiration through a skin patch, where a cholinergic agent is used to stimulate perspiration secretion from the eccrine

sweat gland. Similar perspiration collection devices are described in U.S. Patent No. 5,076,273 to Schoendorfer and U.S. Patent No. 5,140,985 to Schroeder. Detection of extracted glucose is carried out using standard chemical (e.g., enzymatic) colormetric or spectrometric techniques.

5 Alternatively, an iontophoretic transdermal sampling system can be used in conjunction with the present invention, for example where the instant particle method is used to pre-treat a skin site to facilitate improved sampling from a GlucoWatch system (Cygnus, Redwood, CA). This iontophoretic system is described in Gliebfeld *et al* (1989), Pharm. Res. 6(11): 988 *et seq* and US Patent No. 5771890.

10

C. Experimental

Below are examples of specific embodiments for carrying out the methods of the present invention. The examples are offered for illustrative purposes only, and are not intended to limit the scope of the present invention in any way.

15 Efforts have been made to ensure accuracy with respect to numbers used (e.g., amounts, temperatures, etc.), but some experimental error and deviation should, of course, be allowed for.

EXAMPLE 1

Introduction

20 The interstitial fluid is the clear body fluid between cells on the top surface layer of skin. The glucose level in this fluid directly indicates the glucose level in blood. A needleless syringe device can create diffusion pathway into these layers and will allow the collection of a small amount (< 1 ml) of interstitial fluid from which the glucose level can be measured.

25

Materials and Methods

Lactose monohydrate, NF, grade, was obtained from Amresco® (Solon, OH). The lactose powder was sieved to 38-53 µm using U.S. Standard Sieve (Chicago, IL). D-(+) glucose was obtained from Sigma (St. Louis, MO). Human cadaver skin
30 was supplied from New York Firefighter Skin Bank (New York, NY), was pretreated with 80% balanced salt solution, 10% calf serum and 10% glycerol and frozen at the

skin bank. The skin was used as supplied after 1-2 hours thawing at room temperature.

Modified Franz cells (6.9 ml) were designed for investigation of *in vitro* glucose extraction (Fig.1). The donor part in the bottom of the cell was filled with
5 different glucose concentrations ranging from 10-500 mg/dl. The temperature of the glucose solution was maintained at 32°C during the experiments. Human cadaver skin of a thickness of 200-300mm was used. The skin was punched out using a 1 inch (2.54cm) die cutter and placed on the modified Franz cell.

After a few hours for equilibration, 2mg of lactose particles of 38-53µm were
10 filled into tri-laminate cassette of 20 µm polycarbonate membrane and were injected onto the skin tissue using a PowderJect ND1 needleless syringe device fitted with a supersonic nozzle. Device pressure for particle administration was 20 bar. Then, 5µl of hydrogel was placed on the top of the injected skin and a One Touch enzymatic membrane (Lifescan, Milpitas, CA) was contacted with the gel for one minute. The
15 optical density of the membrane was then measured with a Densitometer (Hercules, CA).

Results

Table 1 is a summary of measured optical density of membranes contacted
20 with the donor part (bottom part of the Franz cell) or the hydrogel at the top of the treated skin. As can be seen, the optical density of extracted glucose from the top of the three different skin samples is proportionally increased from 0.04-0.08 to 0.65-0.89 as the optical density of donor part is increased from 0.10 to 0.71. Fig. 2 is the summary plot of optical density from three skin samples over donor part. The
25 correlation (r^2 value) is 0.2 over the three skin samples.

These *in vitro* experimental results demonstrate that there is good correlation ($r^2 = 0.92$) between the measured values of extracted glucose using the particle delivery methods of the present invention and donor compartment which simulated human interstitial fluid.

Table 1: Glucose standard solution and optical density of glucose solution in donor compartment and glucose extracted from three different skin samples

Glucose Standard (mg/dl)	Donor Compartment	Skin 1	Skin 2	Skin 3
10	0.099	0.06	0.04	0.075
50	0.184	0.17	0.19	0.285
100	0.323	0.265	0.325	0.26
250	0.56	0.725	0.665	0.54
500	0.721	-	0.895	0.65

EXAMPLE 2

Introduction

The *in vitro* study with human cadaver skin set out in Example 1 demonstrated that there is a solid correlation of "systemic" glucose levels with fluid samples accessed via a particle delivery method ($r^2 = 0.92$). Therefore, this study was carried out to compare glucose levels from two blood sources (venous blood glucose and capillary blood glucose) with the glucose level of interstitial fluid accessed via a needleless injection device in human subjects.

Additionally, on the needleless injection sites, visual grade of erythema or edema using the Draize scale, change in chromaticity, change in transepidermal water loss (TEWL) and any sensation of pain (VAS) were measured to indicate stratum corneum disruption and confirm particle penetration. Measurements were performed immediately after particle injection and at 24 and 48 hours post-sampling. These measurements profile any correlation between venous glucose, capillary glucose and interstitial glucose with skin tolerability.

Materials and Methods

120 diabetic subjects were included in the study. The subjects were male or female Type I or Type II diabetics of ages 18-70 but excluding diabetics with any skin disorder at the sites of testing, including eczema, psoriasis, etc. or with a history of recurrent skin infections. Sampling sites were antecubital fossa (venous), fingertip (capillary) and volar forearm (particle delivery).

The needleless syringe particle delivery device and compounds were as follows:-

- Powder: lactose, particle size of 20-38 μ m, sieved.
- 10 Cassette: trilaminate with 10 μ m polycarbonate membranes (upstream membrane was slit), 1.0 mg powder payload, prepared and packaged in a clean laboratory environment and terminally sterilised with γ radiation.
- 15 Device: A dermal PowderJect™ ND1 needleless syringe device fitted with a supersonic nozzle, 5cc expansion chamber modified to accommodate trilaminate cassettes, 10 bar compressed air pressure, push button stainless gas cylinder.

The needleless syringe device was held as vertically as possible with the nozzle placed firmly against the skin, ensuring there was no gap between the skin and the end of the device. The device was actuated by pressing down the button at the top.

TEWL and chromaticity were assessed for each volar forearm injection site prior to powder delivery. After the powder was delivered to the site, TEWL was measured for each injection site. Each subject was asked to describe the sensation of administration in a few words and record the sensation on a 100 mm visual analog scale (VAS) for pain, with 100 being the pain of finger-stick and 0 being no pain.

A LifeScan™ glucose detection membrane strip was moistened with 5 μ l of hydrogel and applied to the powder-injected site for 1 minute. The treated sites were swabbed and chromaticity measured for comparison with pre-treatment values.

30 Capillary blood samples were collected by finger stick for glucose analysis using the LifeScan One-Touch system. Blood samples were collected from a vein in the

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antecubital fossa for glucose analysis. The colour intensity of the membranes were quantified with the Bio-Rad densitometer. TEWL and chromaticity of the injected site were measured at 24 and 48 hours post injection.

The protocol used for an oral glucose tolerance test was as follows. All drug therapy that may affect the test was discontinued for at least 3 days before the test. The subjects were instructed to ingest a carbohydrate intake of at least 150 g/day for 3 days before the test, and fast 14 to 15 hours (from 6 pm of the day preceding the test to 8 to 9 am of the day of the test). Test subjects abstained from tobacco, coffee, tea, food, and alcohol during the test. The subjects sat quietly upright during the test. Slow walking was permitted but vigorous exercise was avoided. Before a glucose load was given, Fasting Plasma Glucose (FPG) was measured via the venous, capillary and interstitial glucose sampling techniques described above. 75 g of glucose was given as a 25% solution (400ml). Samples were collected and the capillary and interstitial glucose levels were measured as above at 30, 60, 90, 120 min.

Results

The glucose tolerance test results from three subjects are depicted in Fig. 3 to Fig. 5. The blood glucose concentration (mg/dl) and optical density from reaction with glucose in interstitial fluid are shown. In order to combine the results into the same Figure, optical density was multiplied by 1000.

The dynamic glucose range of subject 1 was 150 to 270 mg/dl. The optical density according to the blood glucose value correlated well with venous glucose concentration (Fig. 3). The dynamic glucose range of subject 2 was 160 mg/dl to 400 mg/dl. There was a correlation between venous glucose and optical density except at the one hour time point (Fig. 4). A similar trend could be observed in subject 3 (Fig. 5).

In Fig. 6, the optical density readings from interstitial fluid glucose were plotted over venous blood glucose of all subjects. The error grid method was applied to the collected data and plotted. Most data points are located in region A and B which are clinically correlated regions. The r value from a linear regression analysis

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was 0.76. Table 2 reports a comparison of error grid analyses between the invasive Glucometer, the iontophoretic GlucoWatch method, and the particle delivery method according to the invention.

5 **Table 2:** Clinical result comparison between Glucometer®, GlucoWatch® and the invention

Zone	Glucometer®	GlucoWatch®	Invention
A	91.3	73.9	77.3
B	7.9	22.7	20.8
C	0	0.06	0
D	0.8	3.41	1.9
E	0	0	0

15 With respect to pain, most subjects (>90%) preferred the particle delivery method according to the invention over the Glucometer and GlucoWatch glucose measuring methods. However, there was some erythema noted in some subjects that resolved after 3-4 days with the methodology of the invention.

20 Accordingly, novel monitoring methods are disclosed. Although preferred embodiments of the subject invention have been described in some detail, it is understood that obvious variations can be made without departing from the spirit and the scope of the invention as defined by the appended claims.

CLAIMS

1. A method for sampling an analyte present beneath a target skin or mucosal surface of an individual, said method comprising:
 - (a) accelerating particles into and/or across said target surface, wherein acceleration of said particles into or across the target surface is effective to allow passage of a fluid sample from beneath the target surface to the target surface; and
 - (b) determining the presence of said analyte in said fluid sample.
2. The method of claim 1 wherein the analyte is a physiologically active material.
3. The method of claim 1 or 2, wherein acceleration of the particles into the target surface in step (a) serves to increase the permeability of the target surface.
4. The method of any one of the preceding claims, wherein the particles are accelerated toward the target surface in step (a) using a needleless syringe device.
5. The method of claim 4, wherein the particles are accelerated toward the target surface at a velocity of about 100 to 2,500 m/sec.
6. The method of any one of the preceding claims, wherein the particles have a size predominantly in the range of about 0.1 to 250 μm .
7. The method of any one of the preceding claims, wherein the particles are coated with a locally active agent.
8. The method of claim 7, wherein the particles are coated with an osmotically active agent or a pharmacological agent.
9. The method of claim 8, wherein the pharmacological agent is a vasoactive agent or an anti-inflammatory agent.
10. The method of any one of the preceding claims, wherein the target surface in step (a) has an overall size ranging from about 0.1 to about 5.0 cm^2 .
11. The method of any one of the preceding claims, wherein the fluid sample comprises interstitial fluid.

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12. The method of any one of the preceding claims wherein step (b) comprise collecting a sample from the target surface.

13. The method of claim 12, wherein the collection step entails contacting the target surface with an absorbent material.

5 14. The method of claim 13, wherein the absorbent material is coated with an enzyme that reacts specifically with the analyte to produce a detectable signal.

15. The method of claim 14, wherein the physiologically active material is glucose and the enzyme is glucose oxidase.

10 16. The method of claim 15, wherein the detectable signal is quantitative and can be correlated with a blood glucose level in the individual.

17. The method of claim 14, wherein the physiologically active material is ethanol and the enzyme is an alcohol oxidase enzyme.

15 18. The method of claim 17, wherein the detectable signal is qualitative and is indicative of the presence or absence of ethanol in the individual or the detectable signal is quantitative and can be correlated with a blood alcohol level in the individual.

19. The method of any one of claims 12 to 18, wherein the sample is collected into a collection means which is contacted with the target surface after the particles are accelerated into said surface.

20 20. The method of any one of claims 12 to 19, wherein the acceleration and collection steps are repeated at least once over the course of a day in order to provide for continual monitoring of the physiologically active material in the individual.

21. The method of any one of the preceding claims wherein step (b) 25 comprises contacting the sample which has passed to the target surface with a sensing apparatus that detects the presence or amount of said analyte.

22. Use of an inert material for the manufacture of a particulate composition for sampling an analyte present beneath a target skin or mucosal surface of an individual by a method comprising:

30 (a) accelerating particles into and/or across said target surface, wherein acceleration of said particles into or

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across the target surface is effective to allow passage of a fluid sample from beneath the target surface to the target surface; and

- (b) determining the presence of said analyte in said fluid sample.

5

Fig.1

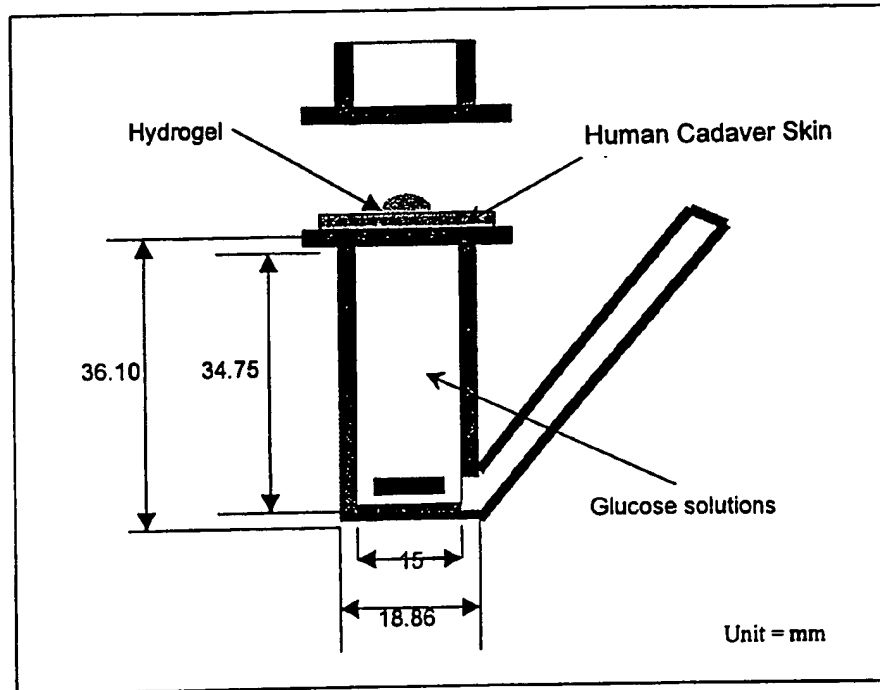


Fig.2

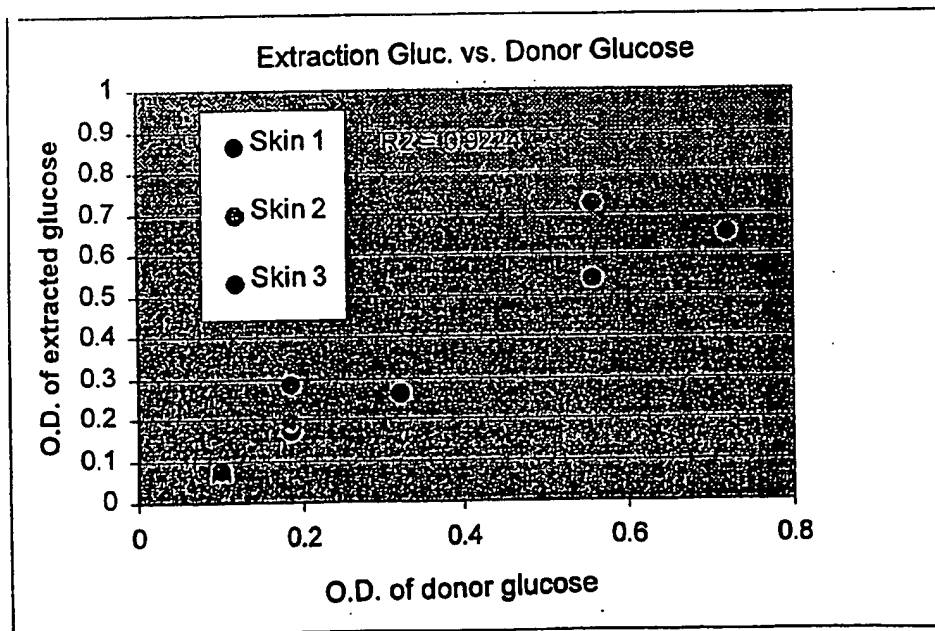


Fig. 3:

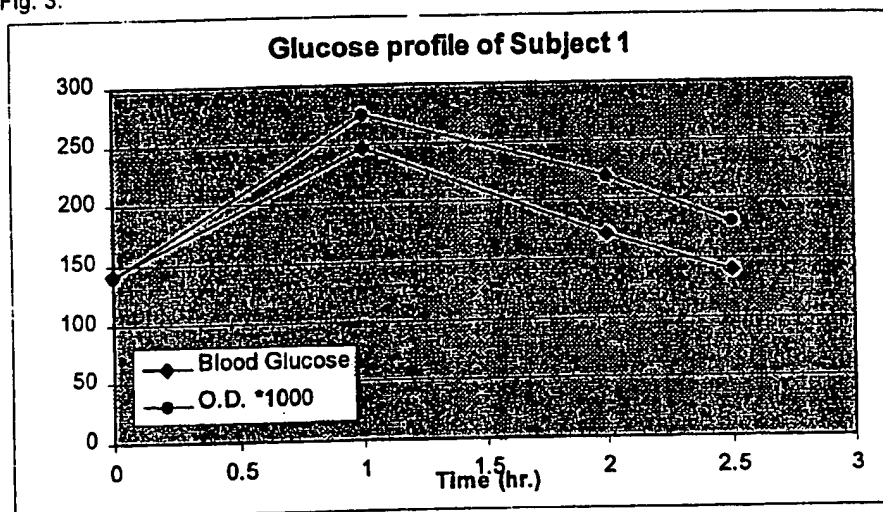
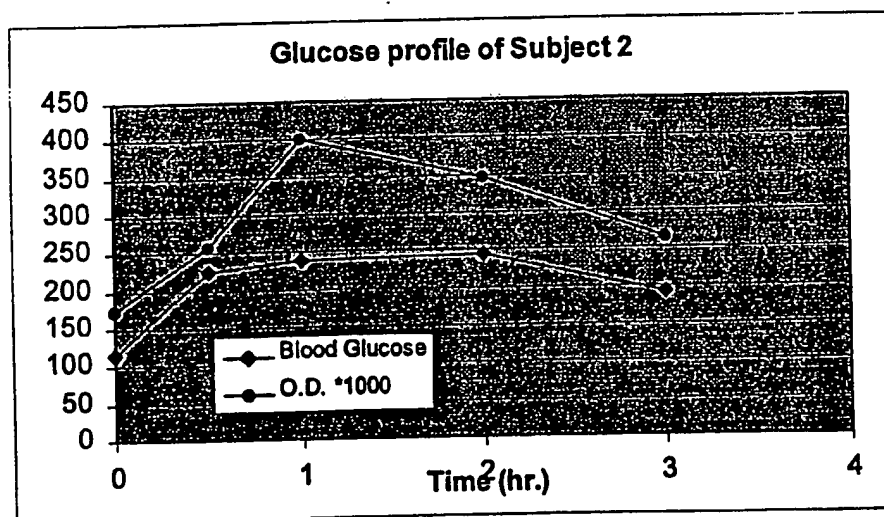


Fig. 4:



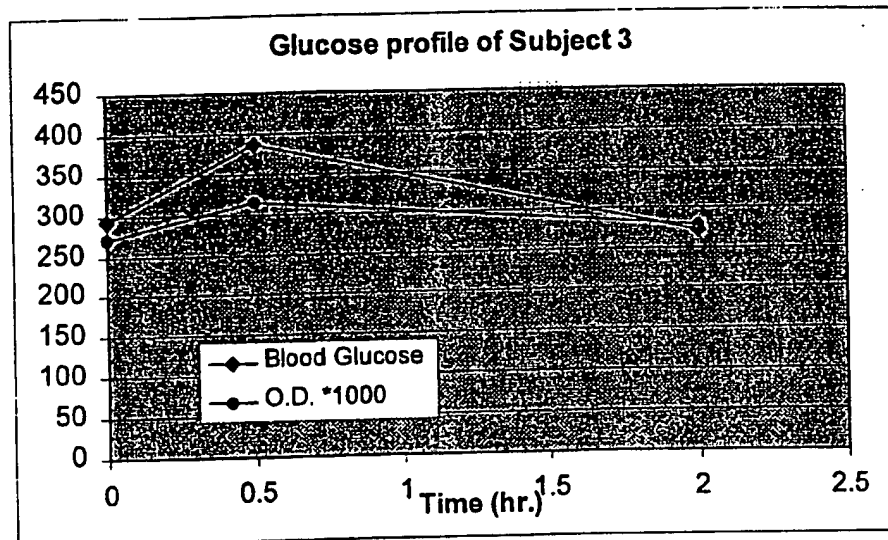
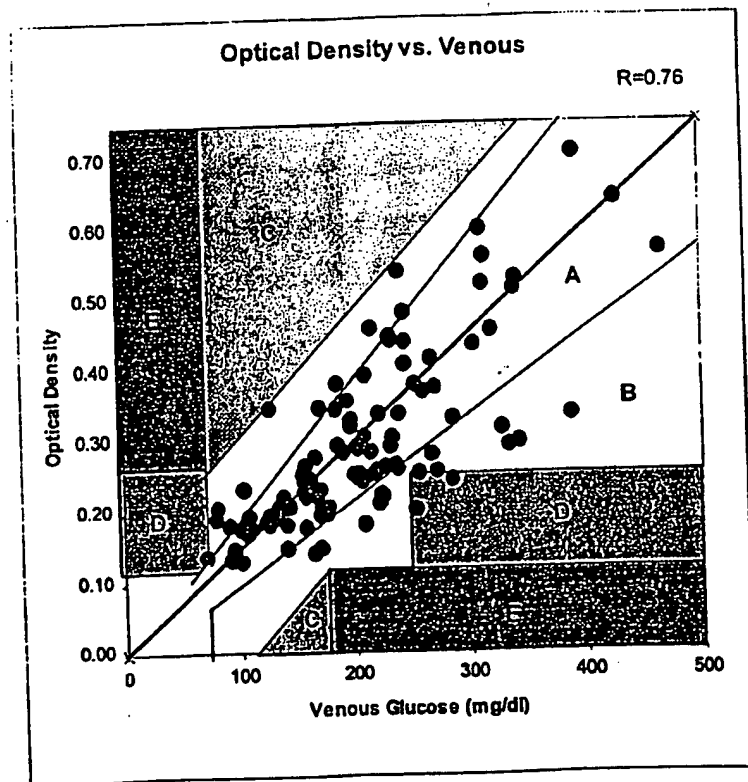


Fig. 5:

Fig. 6



INTERNATIONAL SEARCH REPORT

International Application No
PCT/GB 99/02914

A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 A61B5/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 C12N A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 97 07734 A (EPPSTEIN JONATHAN A ET AL; SPECTRX INC) 6 March 1997 (1997-03-06) page 6, line 30 -page 8, line 12 page 9, line 7 - line 13 page 17, line 7 - line 14 page 58, line 36 -page 59, line 26 page 62, line 27 - line 29	1-3, 11-16 19,21,22
A	WO 94 24263 A (BELLHOUSE BRIAN J ET AL; OXFORD BIOSCIENCE LTD) 27 October 1994 (1994-10-27) cited in the application page 1, line 3 - line 8 page 4, line 1 - line 33 page 5, line 25 - line 35	1,4-7,22
-/-		

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
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- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

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"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

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"&" document member of the same patent family

Date of the actual completion of the international search

2 December 1999

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13/12/1999

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
Fax: (+31-70) 340-3018

Authorized officer

Knüpling, M

INTERNATIONAL SEARCH REPORT

Int'l. Application No
PCT/GB 99/02914

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	<p>SANFORD J C ET AL: "Optimizing the Biolistic Process for Different Biological Applications"</p> <p>METHODS IN ENZYMOLOGY, vol. 217, 1993, pages 483-509, XP002912840</p> <p>sections "Choice of Microprojectiles", "Coating Particles"</p>	1,6,7,22

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